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HST.582J / 6.555J / 16.456J Biomedical Signal and Image Processing  
Spring 2007

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# Introduction to Medical Image Segmentation

HST 582

# Outline

- Applications
- Terminology
- Probability Review
- Intensity-Based Classification
- Prior models
- Morphological Operators

# Applications of Segmentation

- Image Guided Surgery
- Surgical Simulation
- Neuroscience Studies
- Therapy Evaluation

# Interactive Segmentation

MRI image sequence removed due to copyright restrictions.

# Applications of Segmentation

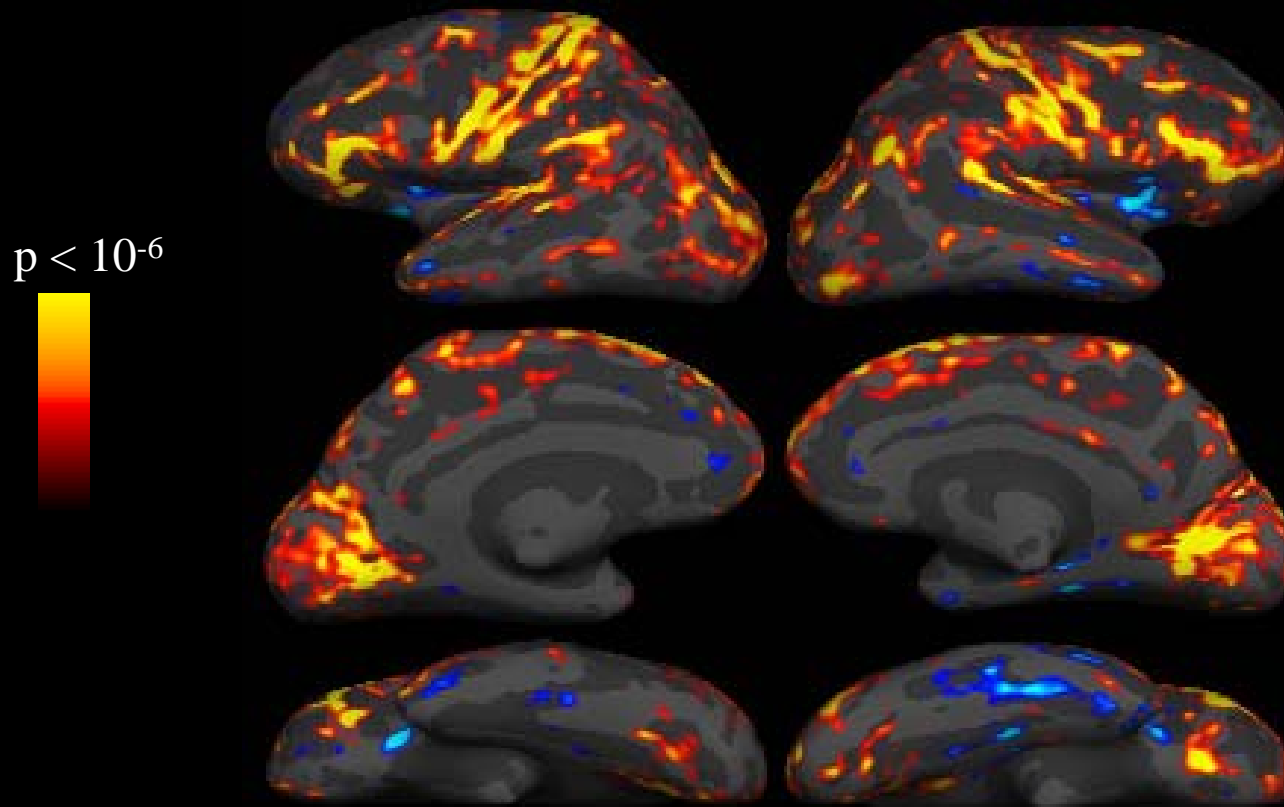
- Image Guided Surgery
- Surgical Simulation

Photo removed due to copyright restrictions.  
Two doctors working with a surgical simulation device.

# Applications of Segmentation

- Neuroscience Studies

# Statistical Map of Cortical Thinning: Aging

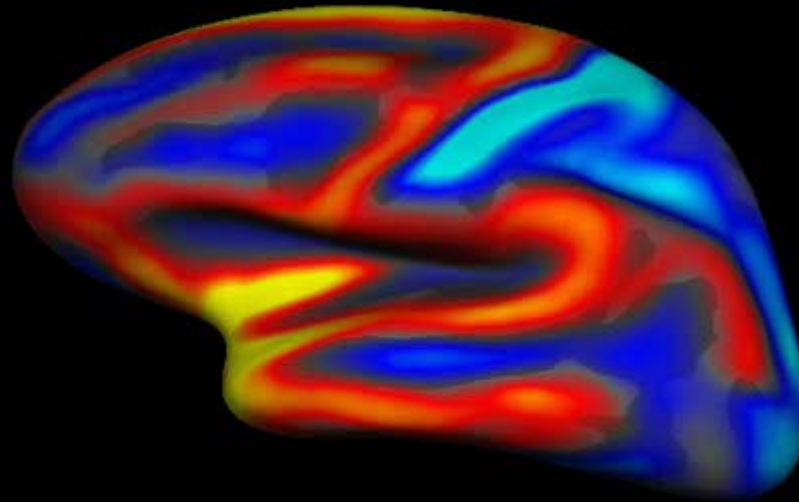


Courtesy of Bruce Fischl. Used with permission.

Thanks to Drs. Randy Buckner and David Salat for supplying this slide.



# Movie of Cortical Thinning with Aging



Courtesy of Bruce Fischl. Used with permission.

2.0 ← 2.25 ← 2.5

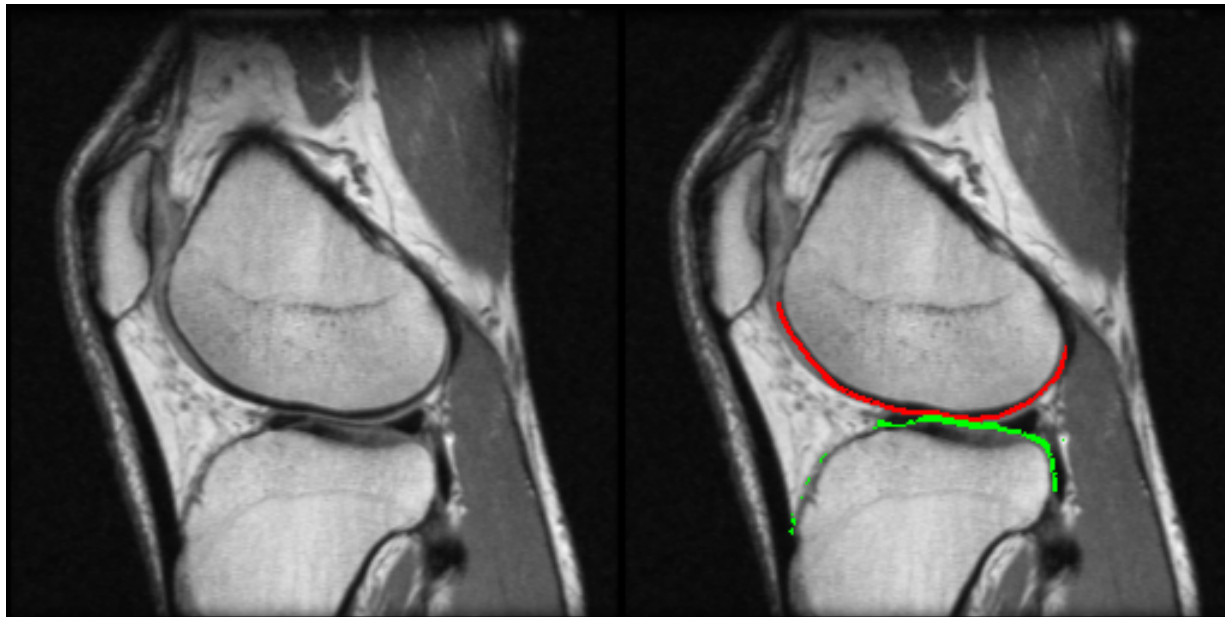
2.5 ← 2.75 ← 3.0



# Applications of Segmentation

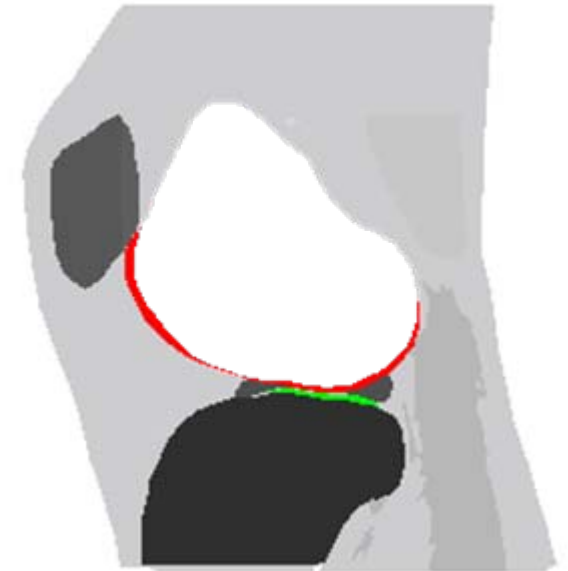
- Therapy Evaluation
  - Multiple Sclerosis
    - Examples Later in talk
  - Knee Cartilage Repair

# Results: Segmentation of Femoral & Tibial Cartilage



MRI Image

Model-Based  
Segmentation



Manual Segmentation

Source: Kapur, Tina. "Model based three dimensional medical image segmentation." MIT Ph.D. thesis, 1999.

Cite as: William (Sandy) Wells. Course materials for HST.582J / 6.555J / 16.456J, Biomedical Signal and Image Processing, Spring 2007.  
MIT OpenCourseWare (<http://ocw.mit.edu>), Massachusetts Institute of Technology. Downloaded on [DD Month YYYY].

# Limitations of Manual Segmentation

- slow (up to 60 hours per scan)
- variable (up to 15% between experts)

[Warfield + 2000]

# The Automatic Segmentation Challenge

An automated segmentation method needs to reconcile

- Gray-level appearance of tissue
- Characteristics of imaging modality
- Geometry of anatomy

# Terminology: *Segmentation*

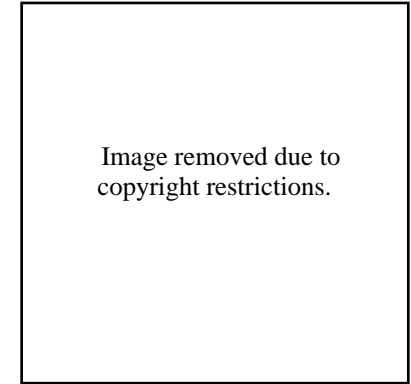
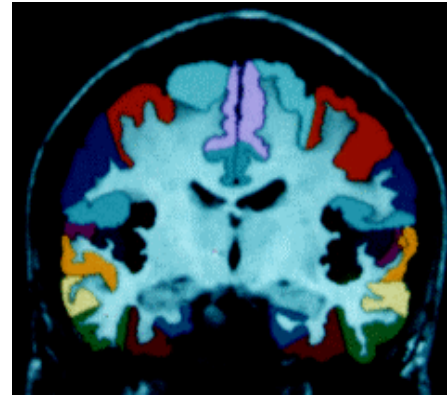
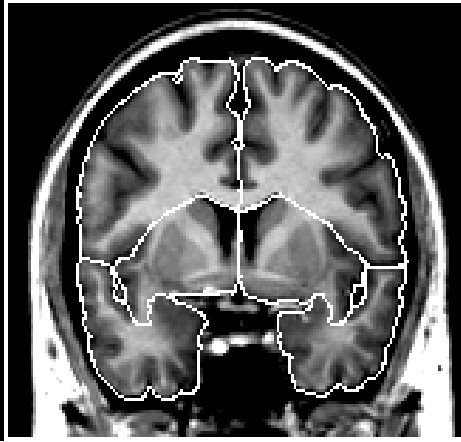
- Graphics Community:
  - Any process that turns images into models
- Another Frequent Usage (HST 582):
  - Labeling images according to tissue type (e.g. White / Gray Matter)
- Another:
  - Dividing imagery into Major Anatomical Subdivisions

# Hierarchical Approach (Brain)

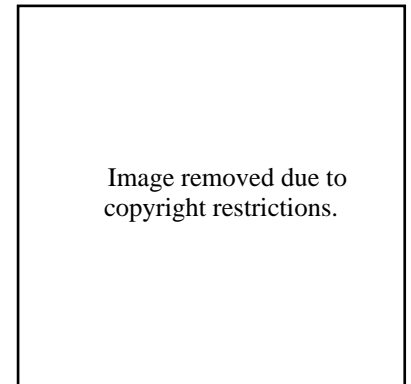
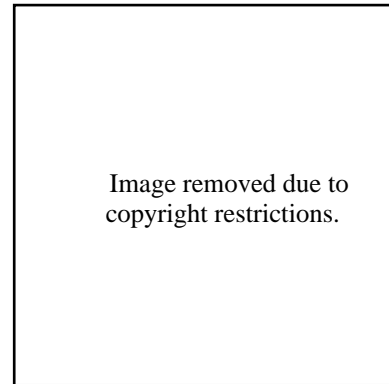
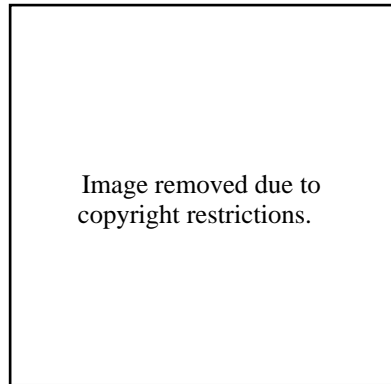
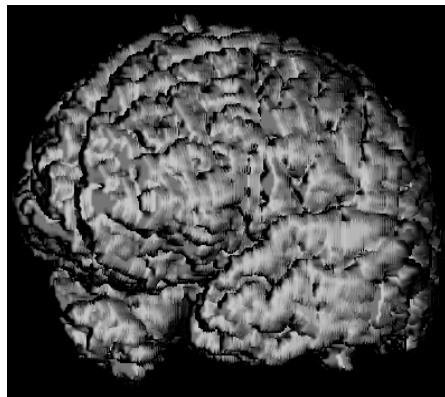
**David Kennedy, MGH / Martinos Center**

- *Segment* into lobes
- *Parcellate* into functional areas

# Neuroanatomic Description Hierarchy:



Courtesy of David N. Kennedy, Ph.D. Used with permission.



## WHOLE BRAIN/STRUCTURE

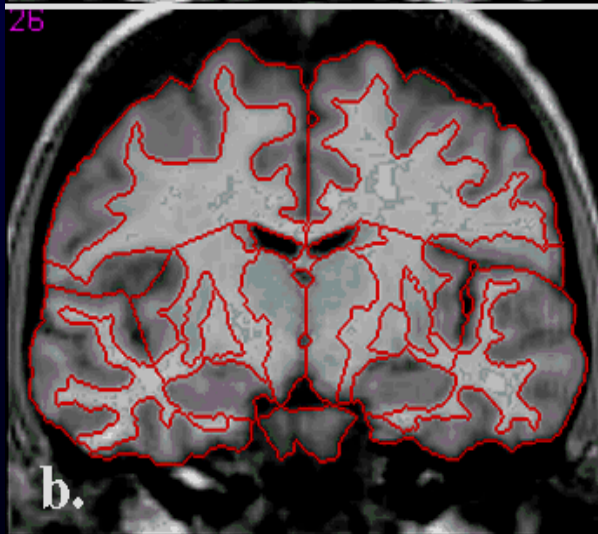
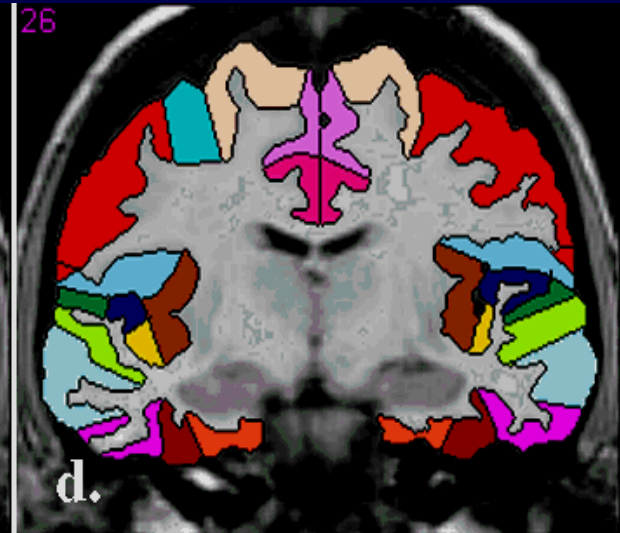
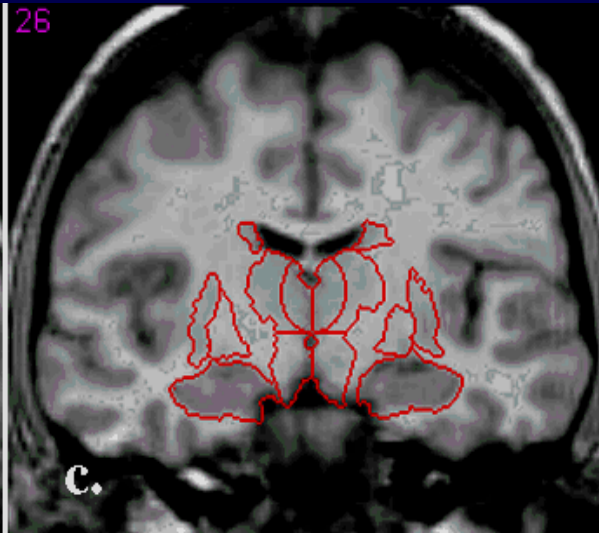
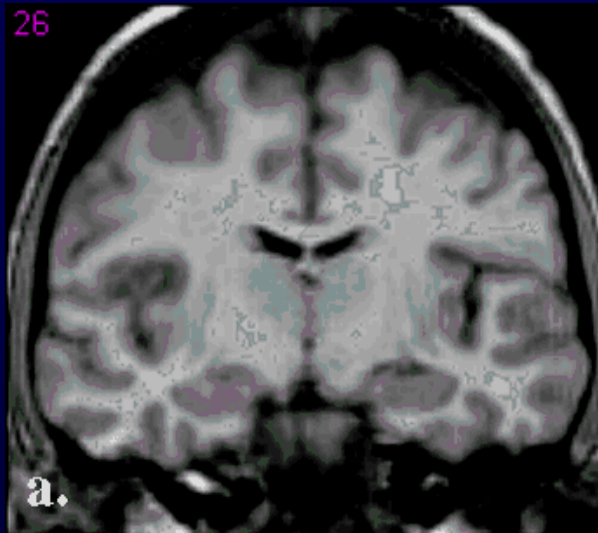


# Stages of Anatomic Analysis

Original

Subcortical Parc.

Cortical Parcellation



“General” Segmentation.

White Matter Parc.

Courtesy of David N. Kennedy, Ph.D. Used with permission.

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# Probability Review

- Discrete Random Variables (RV)
  - Probability Mass Functions (PMF)
- Continuous Random Variables
  - Cumulative Distribution Functions (CDF)
  - Probability Density Functions (PDF)
- Conditional Probability
- Bayes' Rule

# Discrete Random Variable

- Characterized by *Probability Mass Function* (PMF)
  - (sometimes called Distribution)
  - Maps values  $x$  to their Probabilities  $P(x)$

$$0 \leq P(x) \leq 1$$

$$\sum_x P(x) = 1$$

# Continuous Random Variables

- Define Cumulative Distribution Function (CDF) on RV  $\mathbf{x}$

$$F_X(x) = P(X \leq x)$$

$$0 \leq F_X(x) \leq 1$$

- Non-Decreasing
- Sometimes called *Distribution Function*

# Continuous Random Variables...

- Define *Probability Density Function* (PDF)

$$p(x) = \frac{d}{dx}F_X(x)$$

- Easy to show, using Fundamental Theorem of Calculus:

$$P(a \leq x \leq b) = \int_a^b p(x)dx$$

# More on PDFs : $p(x)$

- Non Negative
- Integrates to One
- (Value can be Greater than One)

# Conditional Probability

- Define Conditional Probability:

$$P(X|Y) = \frac{P(X \& Y)}{P(Y)}$$

# Bayes' Rule (easy to show)

$$P(A|B) = \frac{P(B|A)P(A)}{P(B)}$$

- Frequent Situation:
  - A: State of the World
  - B: Measurement
  - $P(B/A)$  : Measurement Model
  - $P(A)$  : A-Priori Model




# Intensity-Based Segmentation

- Statistical Classification
  - ML
  - MAP, a-priori models
  - KNN

# Segmentation

- Easy Segmentation
  - Tissue/Air (except bone in MR)
  - Bone in CT
- Feasible Segmentation
  - White Matter/Gray Matter
  - M.S. Lesions

# Statistical Classification

- Probabilistic model of intensity as a function of (tissue) class
  - Intensity data
  - Prior model
- 
- Classification of voxels

[Duda, Hart 78]

# Measurement Model

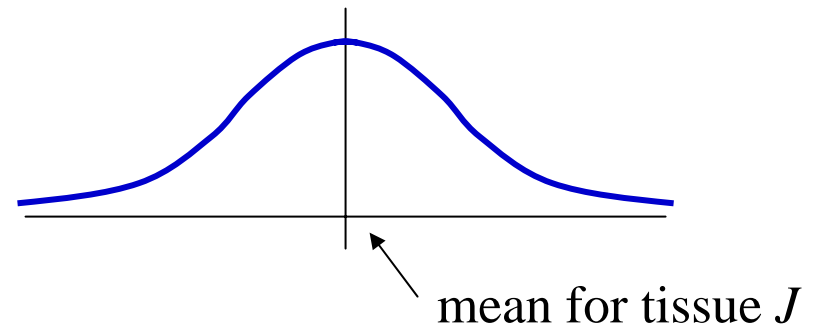
- Characterize sensor

$p(x|\text{tissue class } J)$

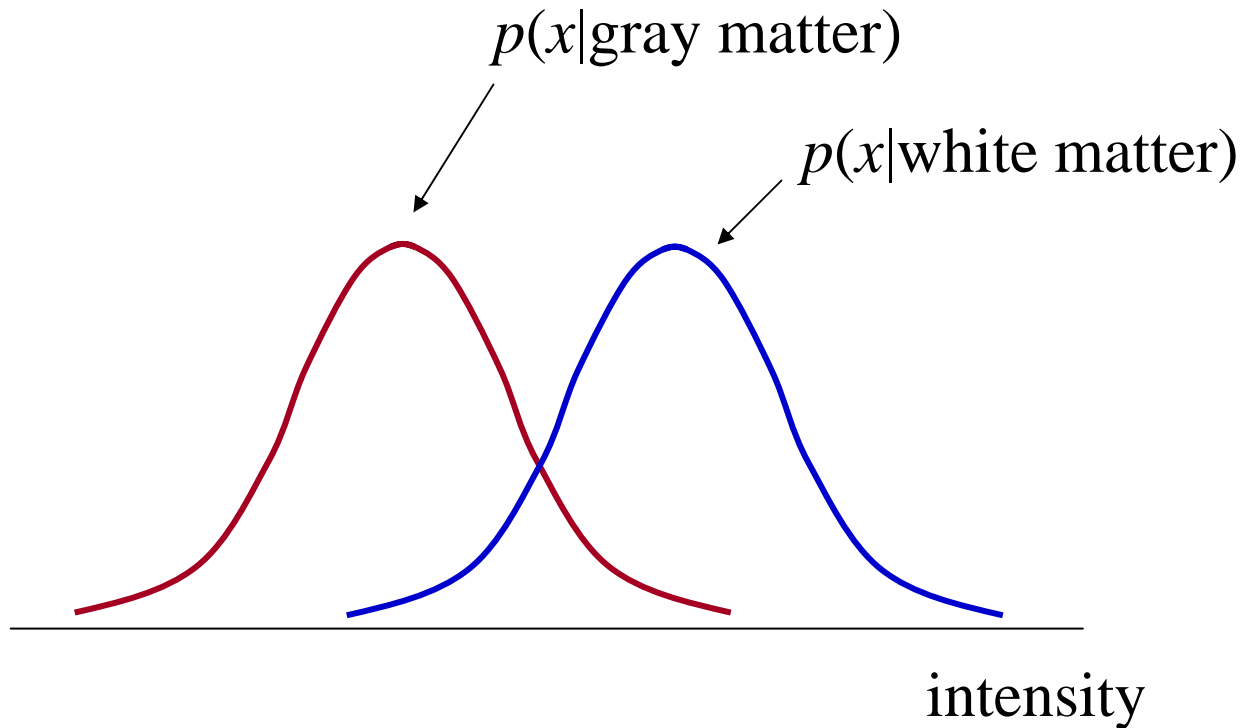
probability density

intensity

Tissue class conditional model  
of signal intensity



# Example



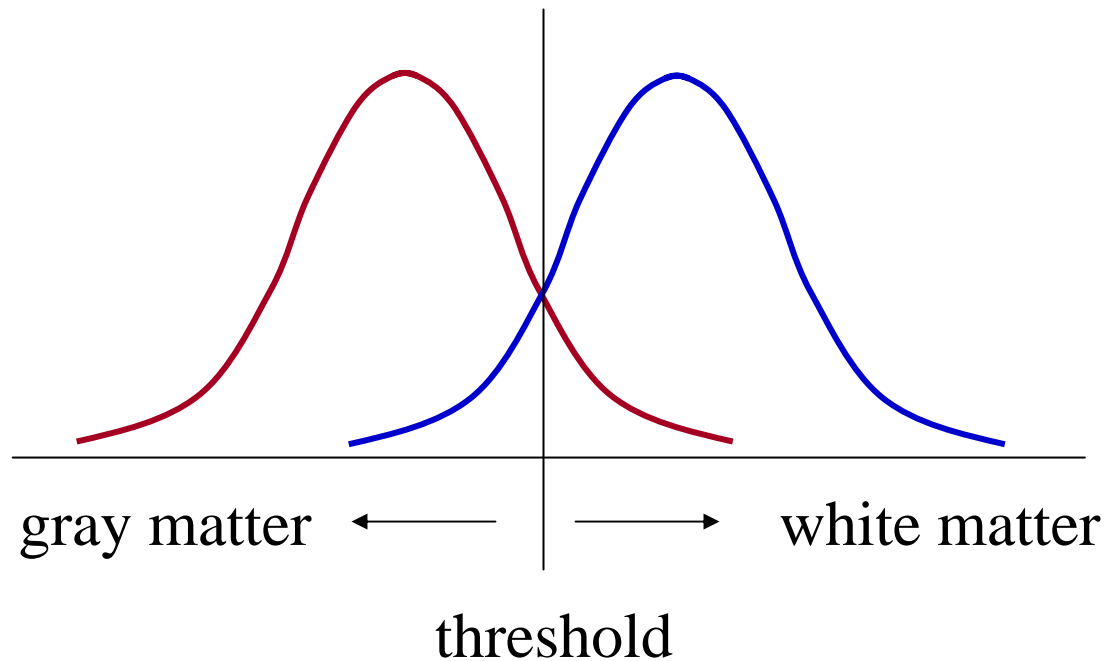
# Maximum Likelihood Classification

- Measure intensity,  $x_o$ , and we want to know the tissue class

$$L(TC_j) = p(x_o | TC_j)$$

- Pick tissue class that maximizes L
- L is not a probability
  - Called: Likelihood

# Example - revisited



# Anatomical Knowledge

- *A priori* model
  - Before the measurement is considered

$$P(TC_j)$$



# MAP Classifier

- Choose TC to Maximize the *A Posteriori* probability

The diagram shows the equation for the Maximum A Posteriori (MAP) classifier,  $P(TC | x_o) = \frac{p(x_o | TC)P(TC)}{p(x_o)}$ , enclosed in a blue-bordered box. Annotations with arrows point to various parts of the equation: 'measurement' points to  $x_o$ , 'model' points to  $p(x_o | TC)$ , 'prior' points to  $P(TC)$ , 'posterior probability' points to the entire left side of the equation, and 'not important' points to the denominator  $p(x_o)$ .

$$P(TC | x_o) = \frac{p(x_o | TC)P(TC)}{p(x_o)}$$

measurement

model

prior

posterior probability

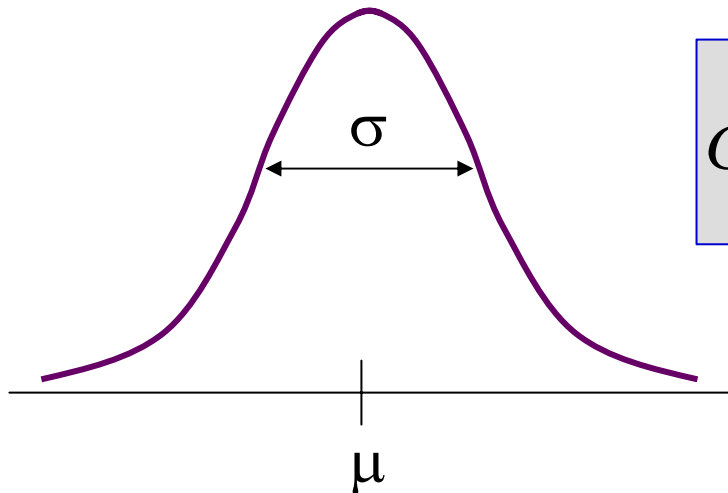
not important

# Measurement Model

- Training data
  - Get an expert to label some of the voxels
- Optional: Use a parametric model
  - Assume functional form
    - Popular choice: Gaussian

# Gaussian Density – 1D

- Why?
  - Central Limit Theorem
  - Makes math easy (when doing parameter estimation)



$$G(\mu, \sigma, x) = \frac{1}{\sqrt{2\pi}\sigma} e^{-\frac{(x-\mu)^2}{2\sigma^2}}$$

# Choosing $\sigma$ and $\mu$

- Use training data:  $\{Y_1, Y_2, \dots, Y_N\}$
- ML parameter estimation

$$\mu = \frac{1}{N} \sum_i Y_i$$

$$\sigma^2 = \frac{1}{N} \sum_i (Y_i - \mu)^2$$

- MAP tissue classifier with Gaussian measurement model: choose tissue class to maximize:

$$P(TC_j | x_o) = \frac{G(\mu_j, \sigma_j, x_o) P(TC_j)}{\dots}$$

# Gaussian Density – 2d Data

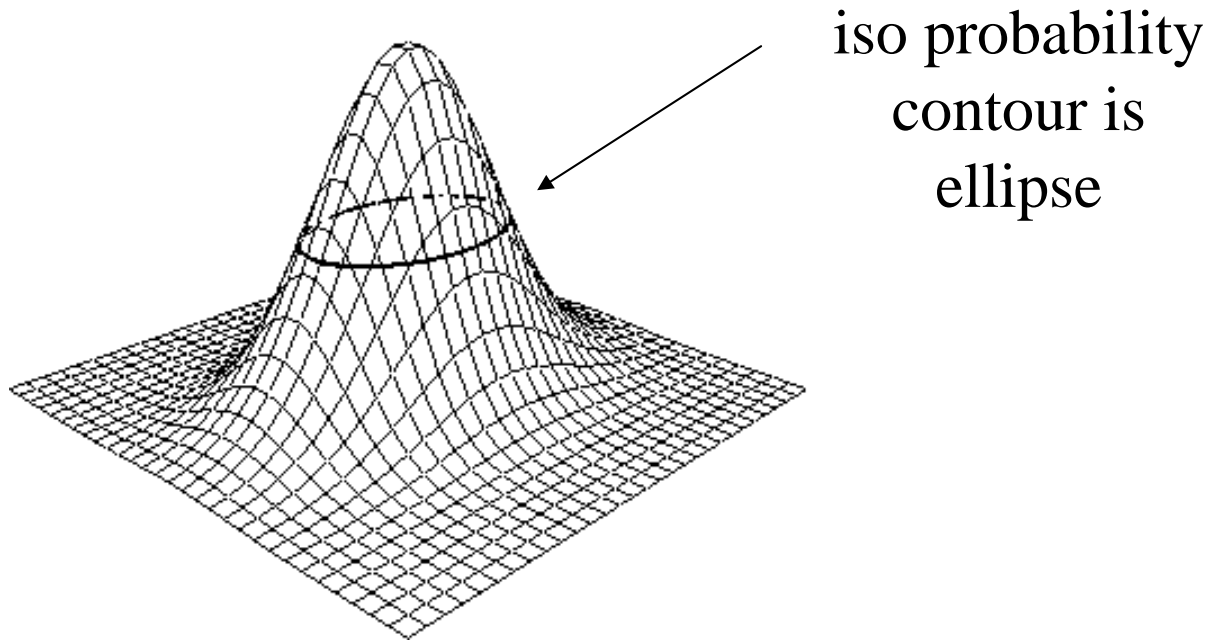
- Example

$$X = \begin{pmatrix} \text{proton density intensity} \\ \text{T2 weighted intensity} \end{pmatrix}$$

Vector Gaussian

$$G(M, \Sigma, X) = \frac{1}{(2\pi)^{\frac{N}{2}} |\Sigma|^{\frac{1}{2}}} e^{-\frac{1}{2}(X-M)^T \Sigma^{-1} (X-M)}$$

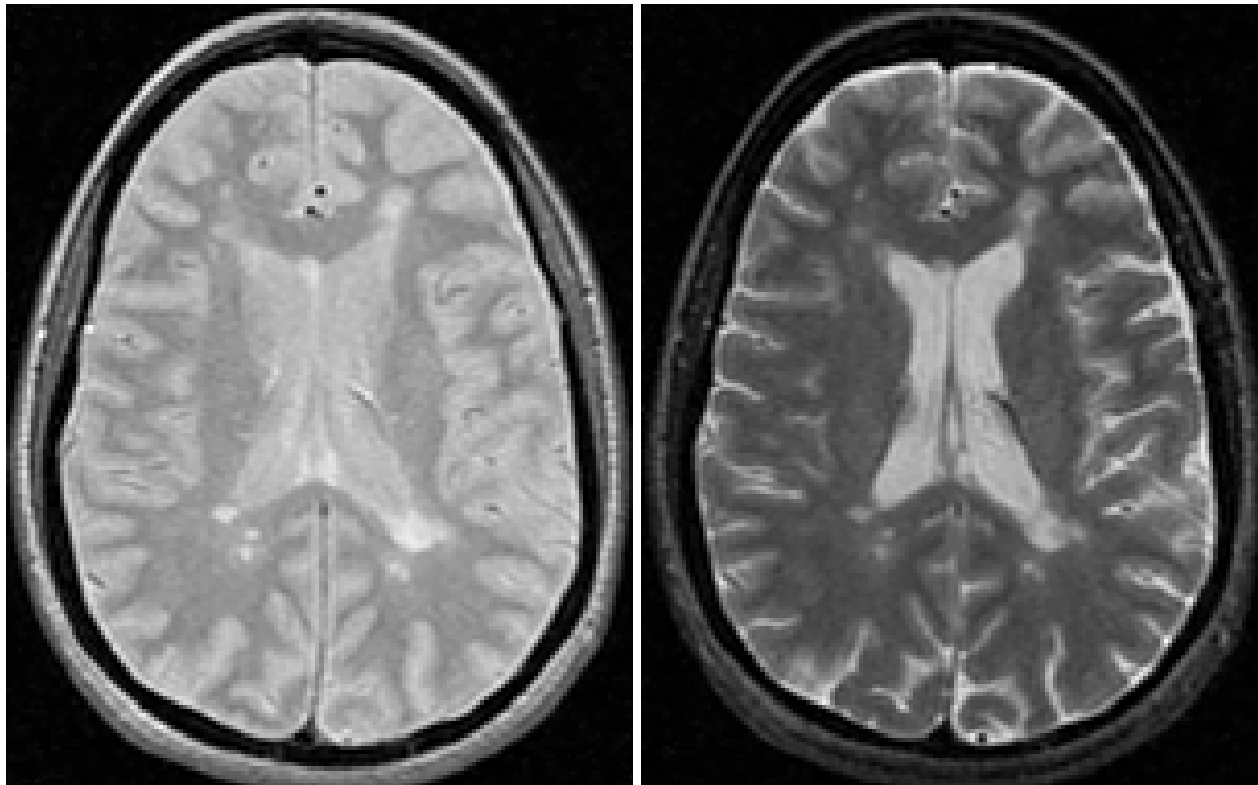
# 2D Gaussian: Example



# Multiple Sclerosis Example

- Dual echo MRI
  - 1 x 1 x 3 mm
  - Registered slice pairs
- Proton density image
  - Good: white/gray
  - Bad: gray/csf
- T2-weighted image
  - Good: CSF/
  - Not so good: white/gray
  - Good: MS lesions

# Multiple Sclerosis



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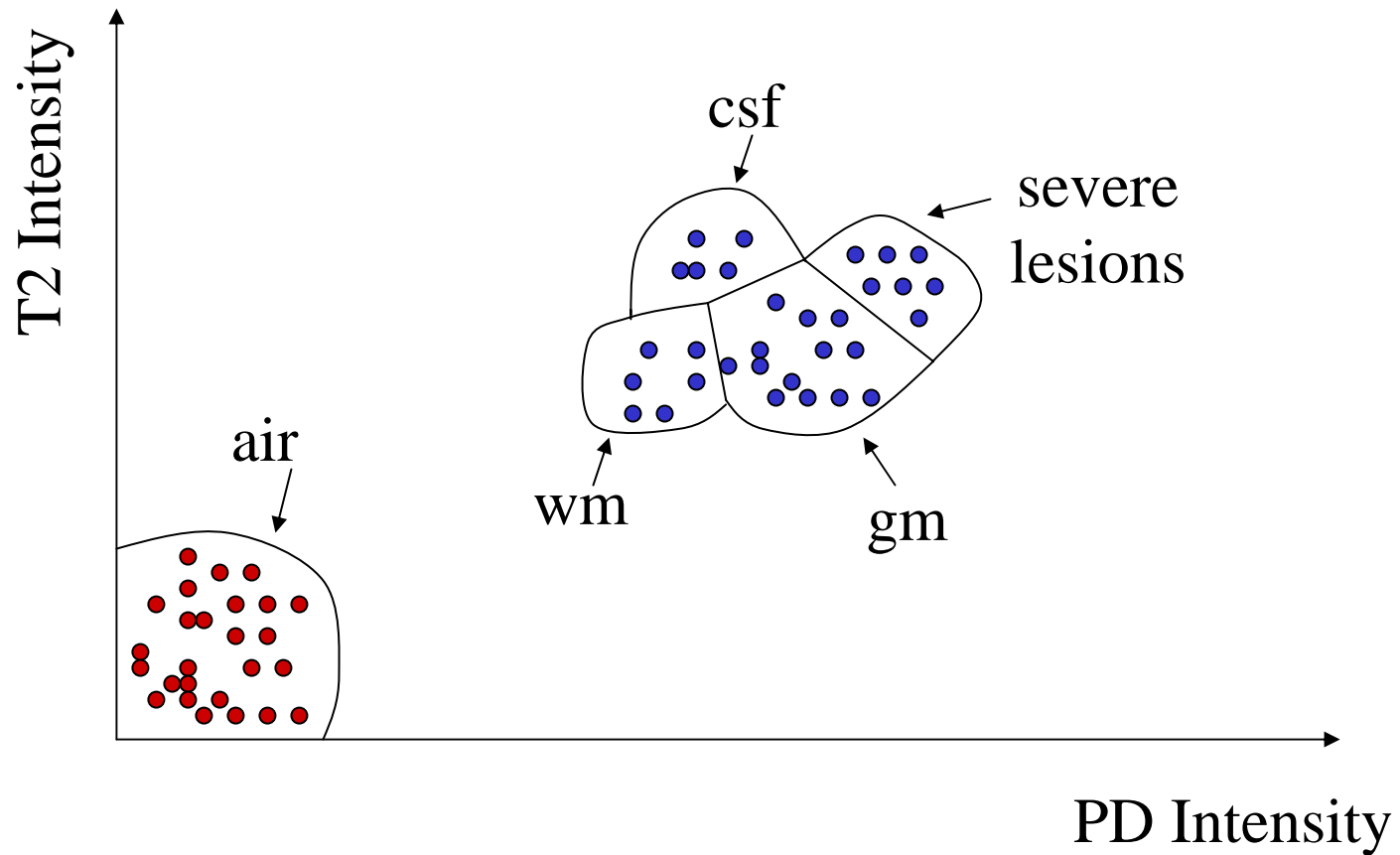
PDw

T2w

Provided by S Warfield

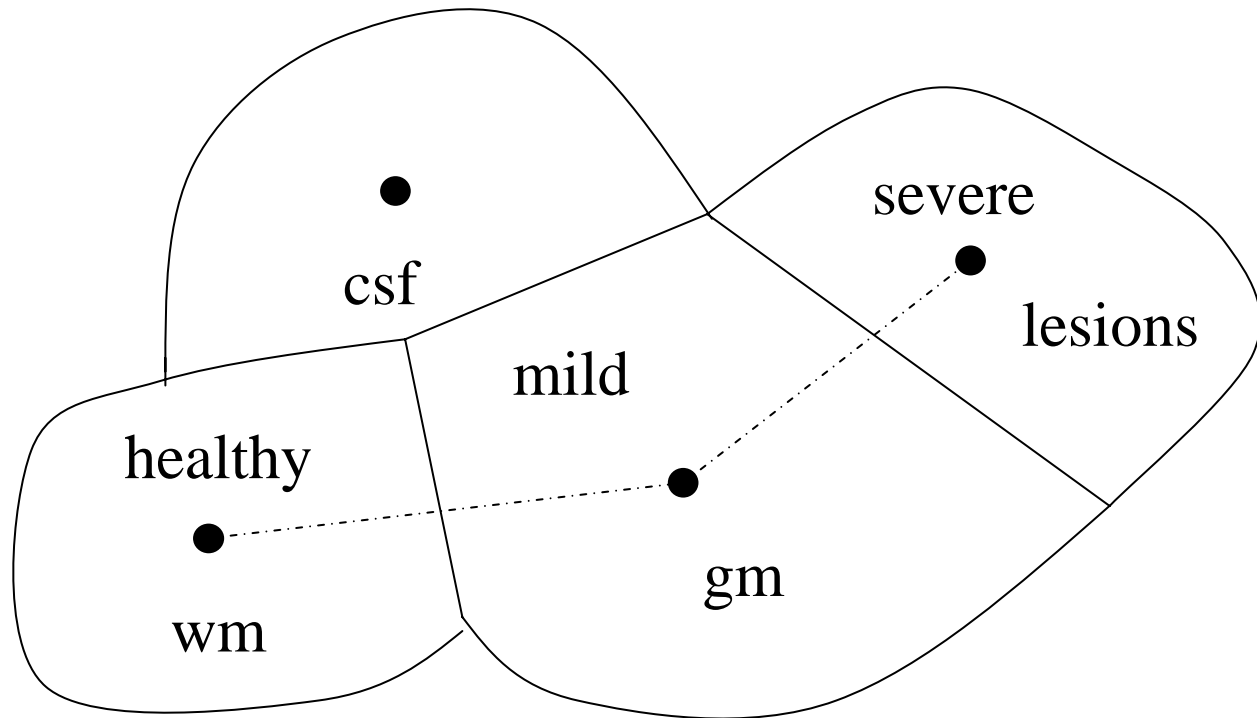


# Dual Echo MRI Feature Space

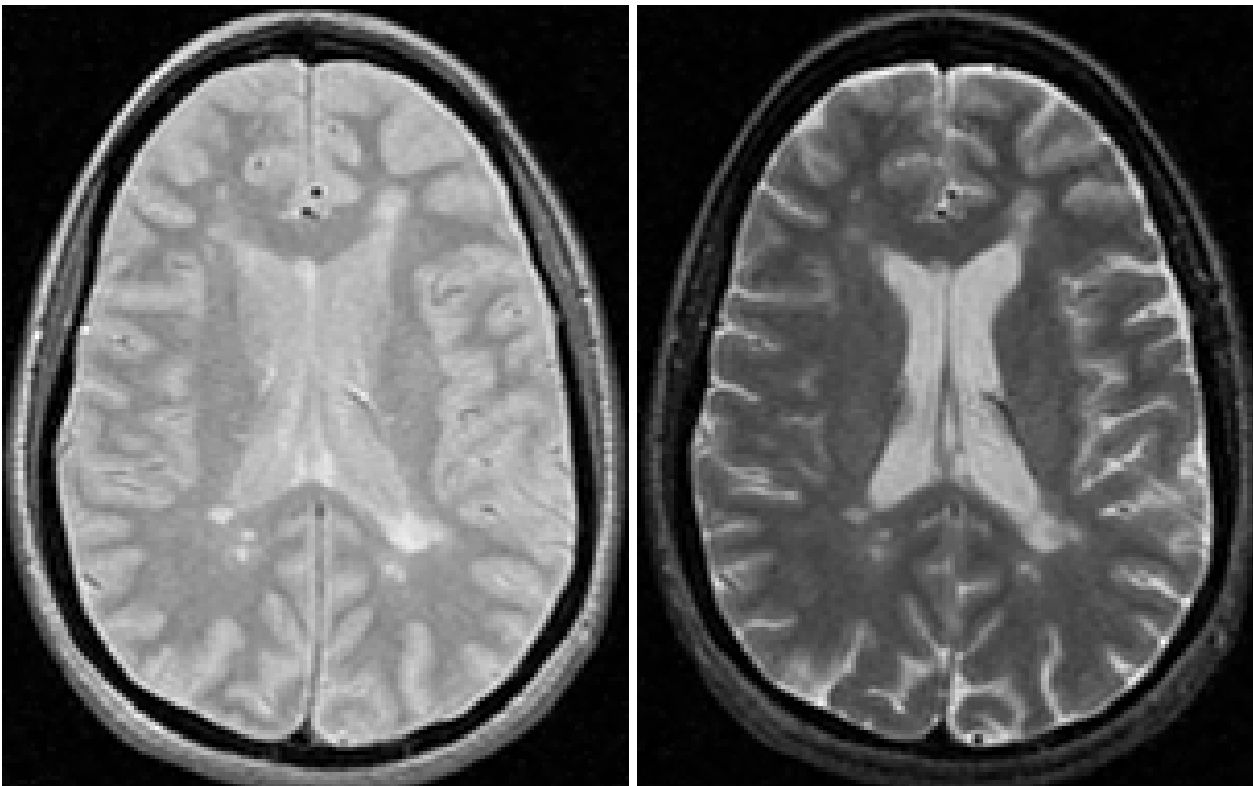


# Detail

- MS Lesions are “graded phenomenon” in MRI, and can be anywhere on the curve



# Multiple Sclerosis



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PDw

T2w

Segmentation

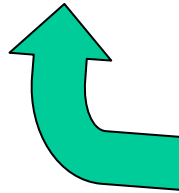
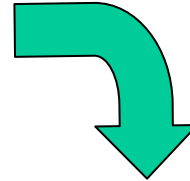
# Background: Intensity Inhomogeneities in MRI

- MRI signal derived from RF signals...
- Intra Scan Inhomogeneities
  - “Shading” ... from coil imperfections
  - interaction with tissue?
- Inter Scan Inhomogeneities
  - Auto Tune
  - Equipment Upgrades

# EM-Segmentation

E-Step

Compute tissue posteriors  
using current intensity  
correction.



Estimate intensity correction  
using residuals based on  
current posteriors.

M-Step

Provided by T Kapur

# Dual Echo Longitudinal Study

Images from Dr. Simon Warfield removed due to copyright restrictions.

PDw

T2w

# Tissue classification

Images from Dr. Simon Warfield removed due to copyright restrictions.

No Intensity Correction

EM Segmentation

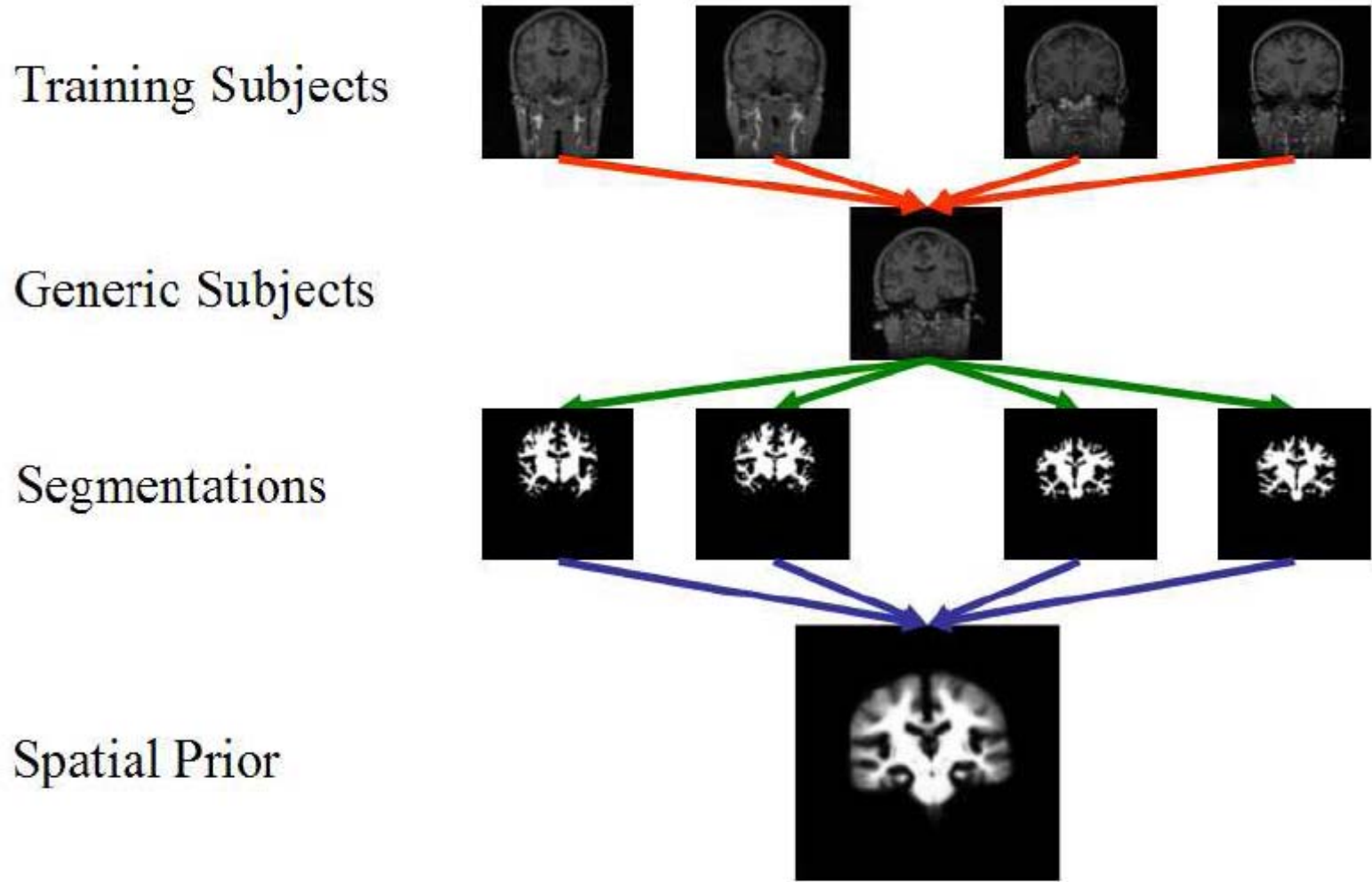
# Prior Models

- Average Brain
- Structurally-Conditioned Models
- Markov Random Fields (MRF)
  - Ising
  - Potts



# Average Brain Models

- Construct a spatial prior model by averaging tissue distributions over a population [MNI].



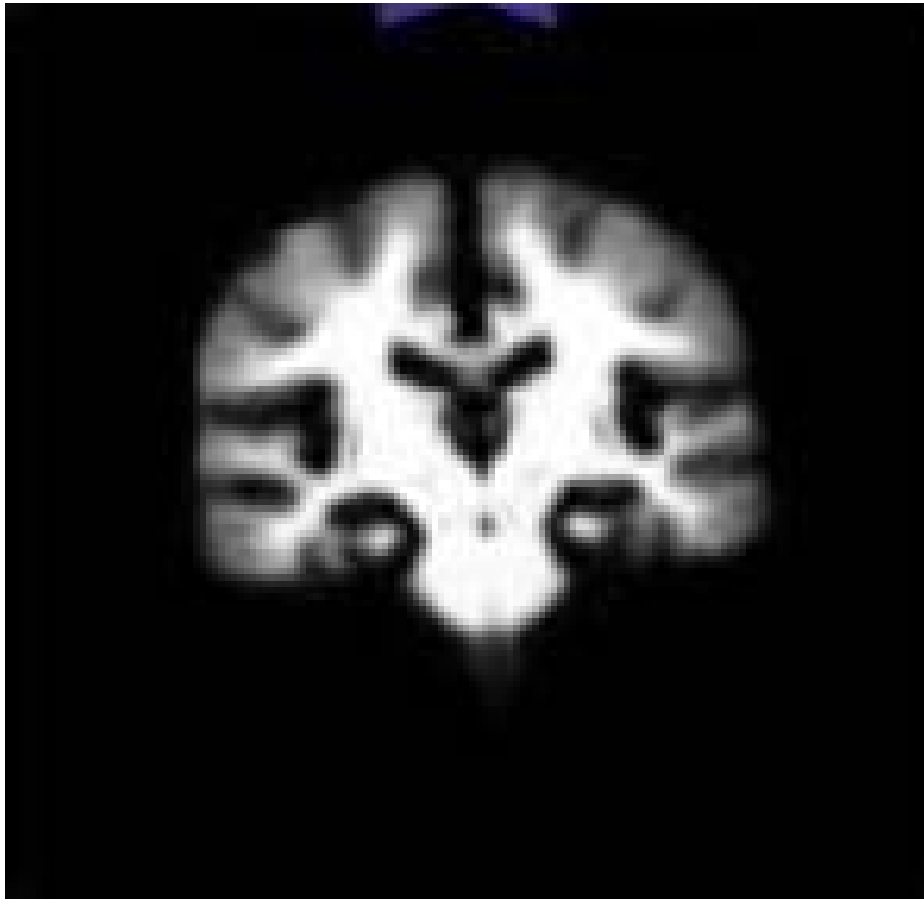
→ register MRIs   
 → align Segmentation   
 → produce prior

**Provided by Kilian Pohl**

Source: Pohl, Kilian M. "Prior Information for Brain Parcellation." MIT Ph.D. thesis, 2005.

Cite as: William (Sandy) Wells. Course materials for HST.582J / 6.555J / 16.456J, Biomedical Signal and Image Processing, Spring 2007. MIT OpenCourseWare (<http://ocw.mit.edu>), Massachusetts Institute of Technology. Downloaded on [DD Month YYYY].

# $P(\text{white matter} \mid x \ y)$



**Provided by Kilian Pohl**

Source: Pohl, Kilian M. "Prior Information for Brain Parcellation." MIT Ph.D. thesis, 2005.

Cite as: William (Sandy) Wells. Course materials for HST.582J / 6.555J / 16.456J, Biomedical Signal and Image Processing, Spring 2007. MIT OpenCourseWare (<http://ocw.mit.edu>), Massachusetts Institute of Technology. Downloaded on [DD Month YYYY].

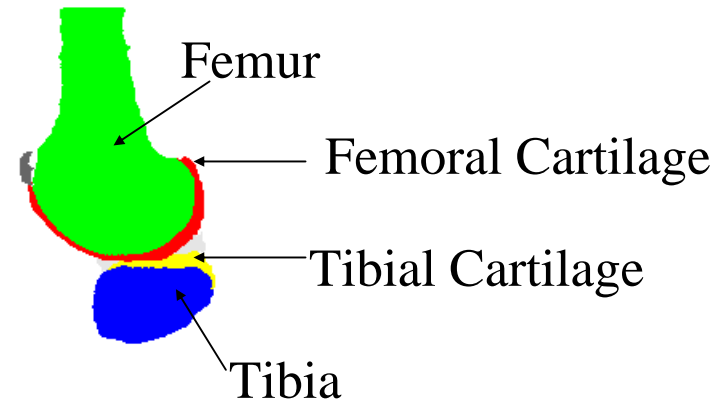
# Structurally-Conditioned Prior Models

- From (Kapur 1999)
  - Modeling Global Geometric Relationships between Structures

# Modeling Global Geometric Relationships between Structures

- Relative Geometry Models
- Motivate Using Knee MRI
- Brain MRI Example

# Segmented Knee MRI



Source: Kapur, Tina. "Model based three dimensional medical image segmentation." MIT Ph.D. thesis, 1999.

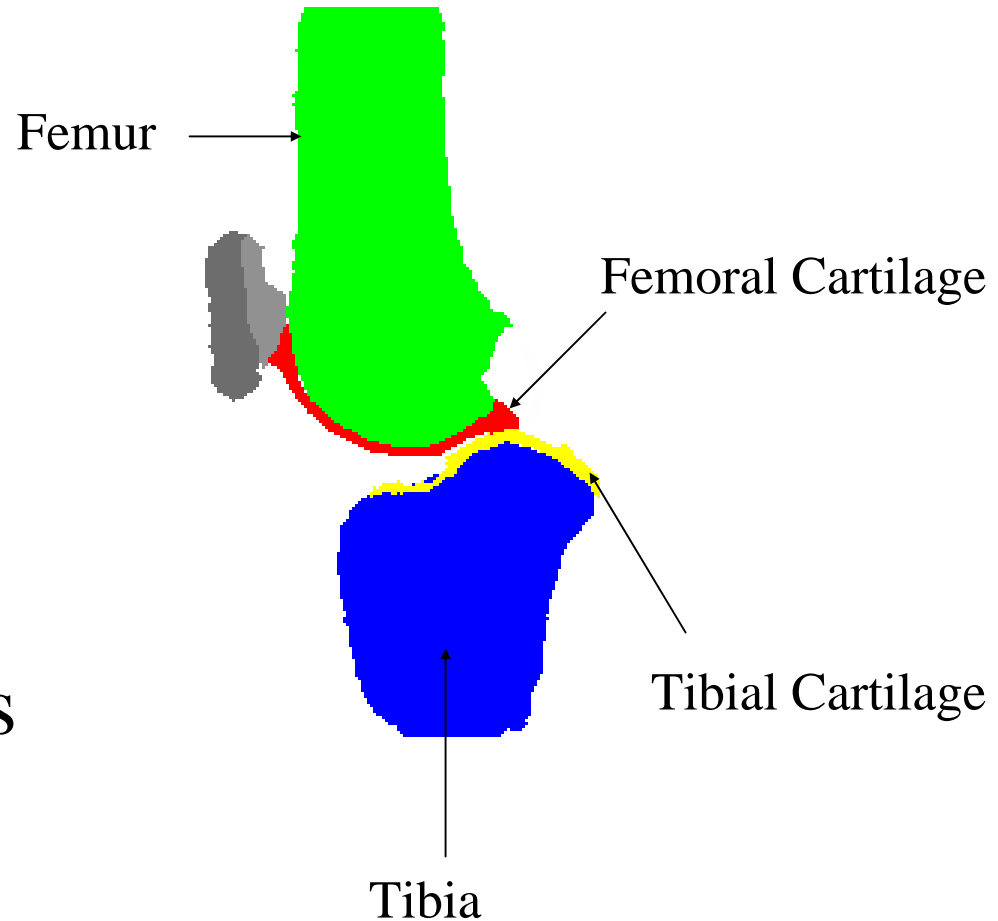
# Motivation

- **Primary Structures**

- image well
- easy to segment

- **Secondary Structures**

- image poorly
- relative to primary



Source: Kapur, Tina. "Model based three dimensional medical image segmentation." MIT Ph.D. thesis, 1999.

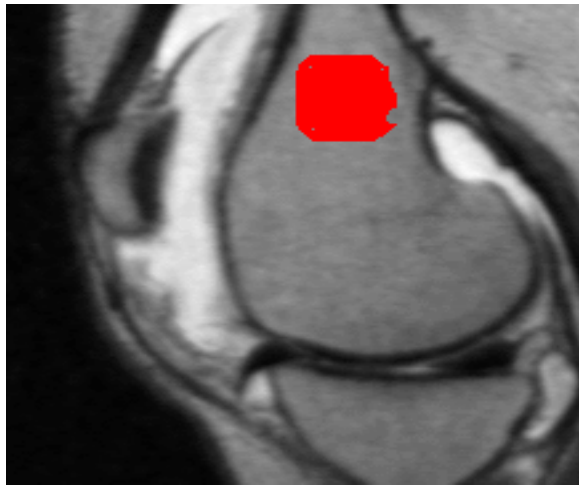
# Relative Geometric Prior Approach

- Select primary/secondary structures
- Measure geometric relation between primary and secondary structures from training data
- Given novel image
  - segment primary structures
  - use geometric relation as prior on secondary structure in EM-MF Segmentation

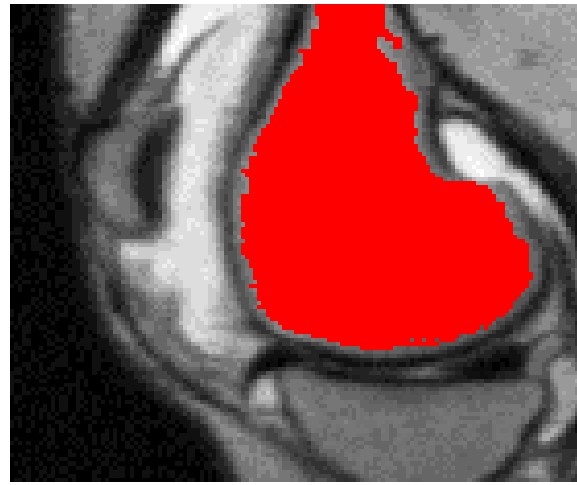
Provided by T Kapur



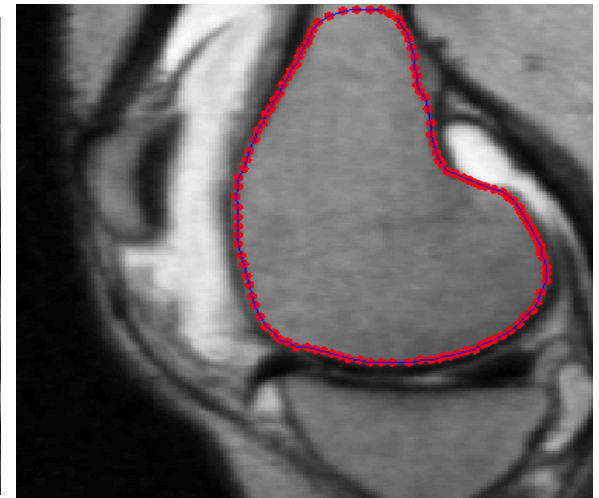
# Segment Primary Structures: Femur, Tibia



Seed



Region Growing



Boundary Localization

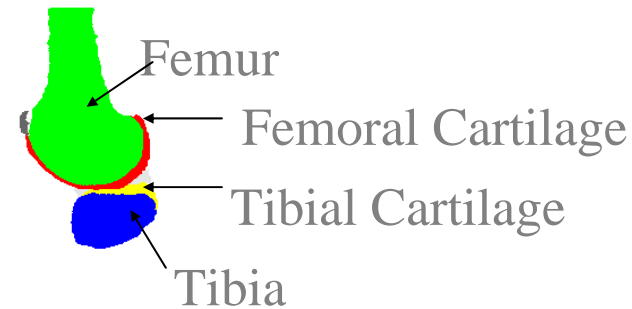
Source: Kapur, Tina. "Model based three dimensional medical image segmentation." MIT Ph.D. thesis, 1999.

# Status

- Have Bone
- Want Cartilage

Provided by T Kapur

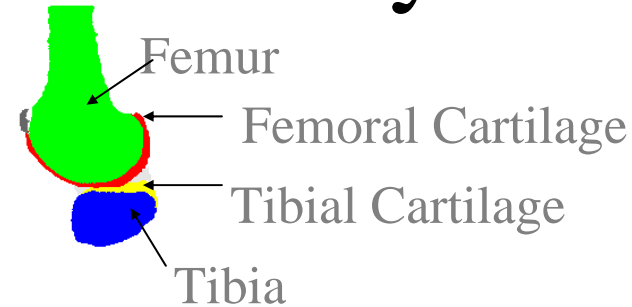
# Measure Geometric Relationship between Primary and Secondary Structures



- Using primitives such as
  - distances between surfaces
  - local normals of primary structures
  - local curvature of primary structures
  - etc.

Provided by T Kapur

# Measure Geometric Relationship between Primary and Secondary Structures



$\rho_s \equiv$  distance to closest point on bone (femur)

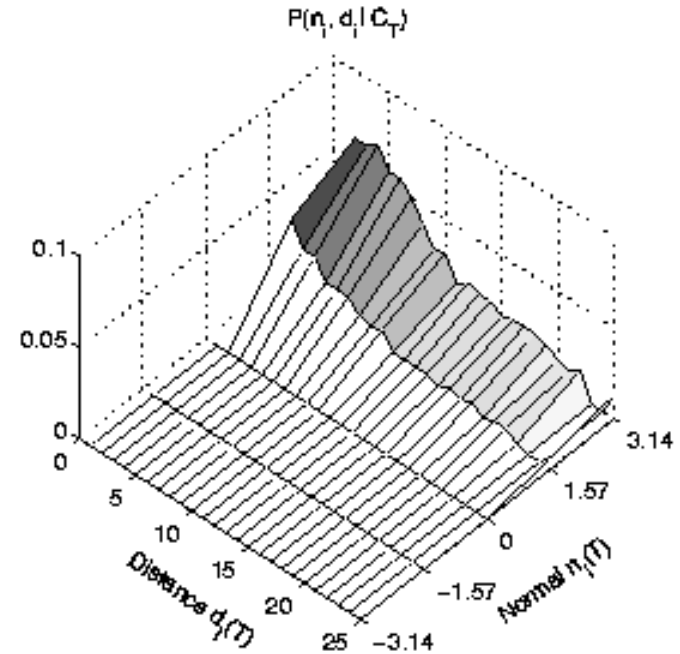
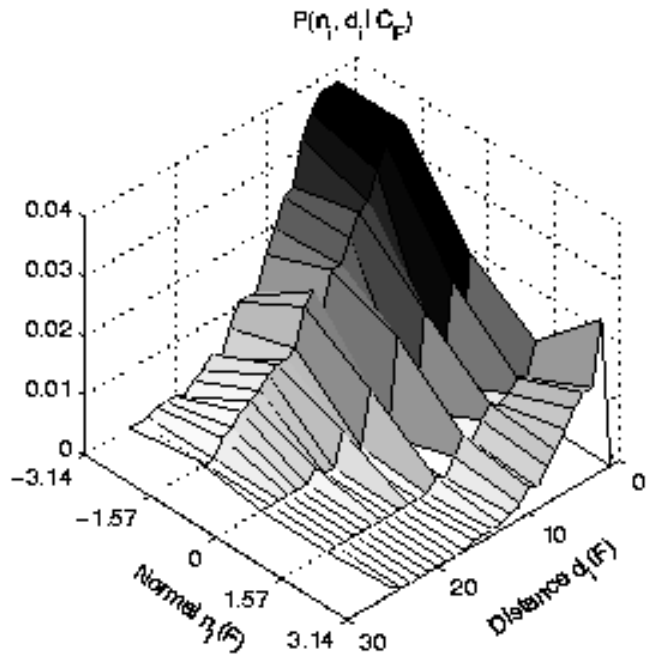
$n_s \equiv$  normal to bone (femur) at closest point

$P(x_s \in \text{Cartilage} \mid \text{Bone})$

$$\approx \frac{P(\rho_s, n_s \mid x_s \in \text{Cartilage})P(\text{Cartilage})}{Z}$$

Provided by T Kapur

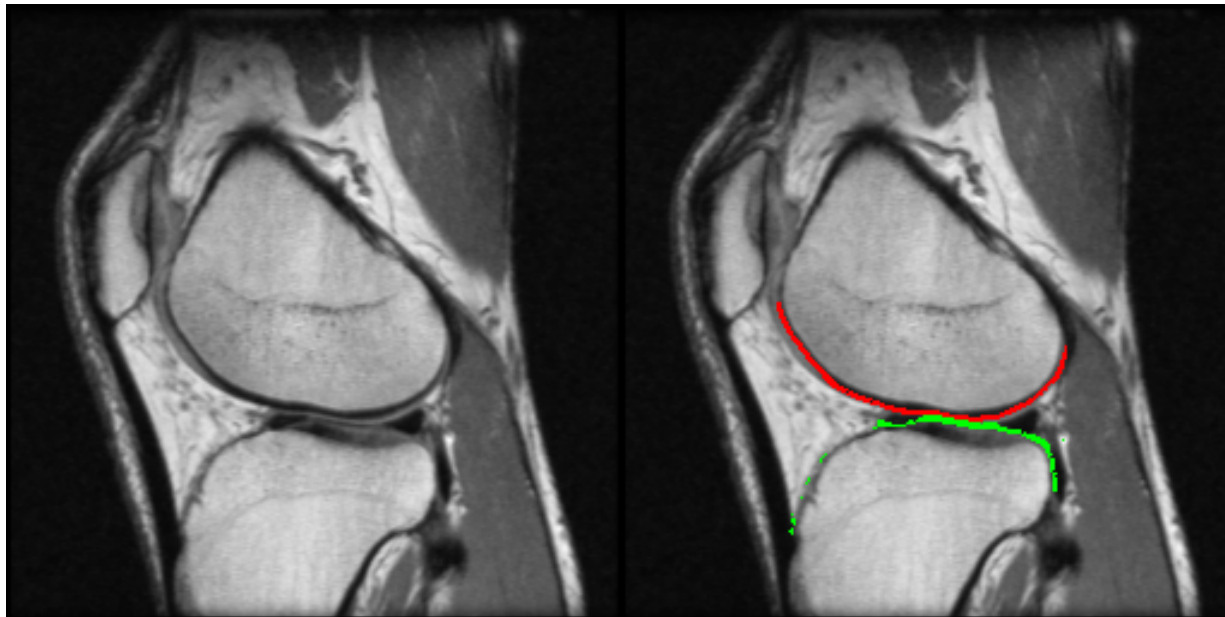
# Estimate of $P(\rho_s, n_s | x_s \in \text{Cartilage})$



$P(\rho_s, n_s | x_s \in \text{Fem. Cartilage})$     $P(\rho_s, n_s | x_s \in \text{Tib. Cartilage})$

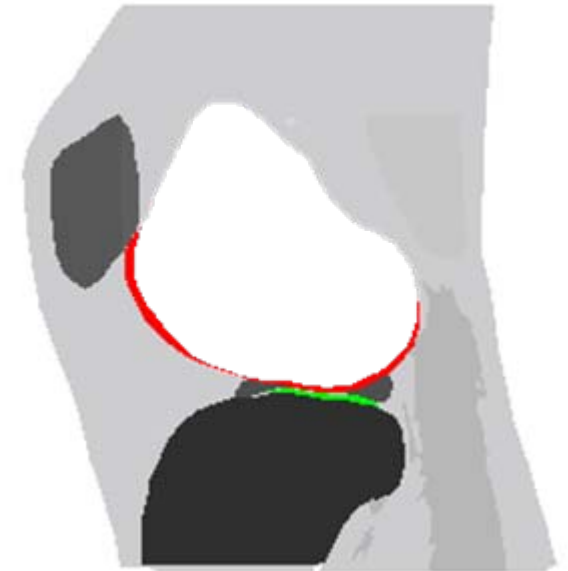
Source: Kapur, Tina. "Model based three dimensional medical image segmentation." MIT Ph.D. thesis, 1999.

# Results: Segmentation of Femoral & Tibial Cartilage



MRI Image

Model-Based  
Segmentation



Manual Segmentation

Source: Kapur, Tina. "Model based three dimensional medical image segmentation." MIT Ph.D. thesis, 1999.

# kNN combined with Atlas

- Simon Warfield
- Use Atlas to control kNN Classifier
  - Resolve contrast failure

# Overlapping distributions

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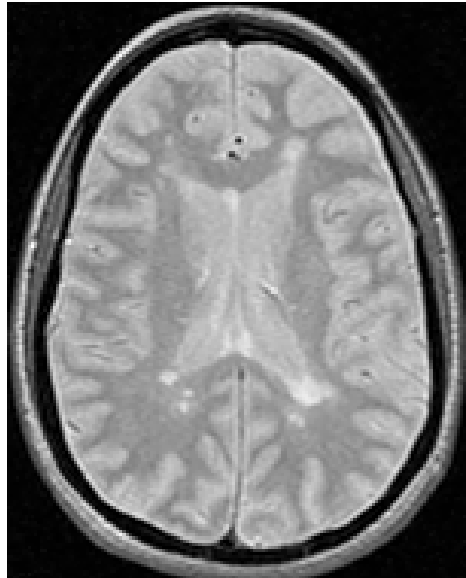
# Lesion classification

Images from Dr. Simon Warfield removed due to copyright restrictions.

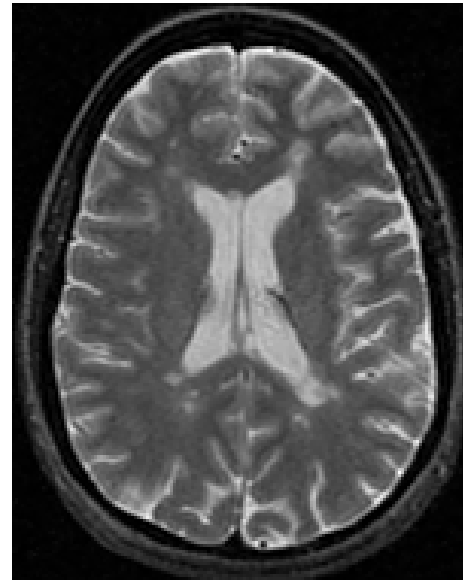
# Lesion classification

Images from Dr. Simon Warfield removed due to copyright restrictions.

# Multiple Sclerosis



PDw



T2w

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# Morphological Operations

- Erosion
- Dilation
- Opening
- Closing
  
- [Haralick + 1989]

# Morphological Operators...

- Ubiquitous simple tools. Useful for ad-hoc clean-up of results from Statistical Classification.

# Dilation

- Binary (or Boolean) images
- Represent image by a set of coordinate vectors of pixels with value 1

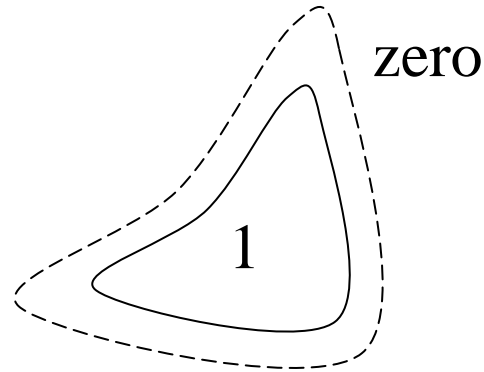
image  $\rightarrow A \oplus B \equiv \{c \mid c = a + b, \text{ for some } a \in A, b \in B\}$

vector addition

Typical structure elements:  $\left\{ \begin{array}{cc} 1 & 1 \\ 1 & 1 \end{array} \right.$   $\begin{array}{ccc} & & 1 \\ 1 & 1 & 1 \\ & & 1 \end{array}$

# Dilation

- Continuous analogy
- Makes structures *fatter*



# Erosion

- Erosion is dual of dilation
  - complement A
  - reflect B (negate coordinates)
  - dilate
  - complement result

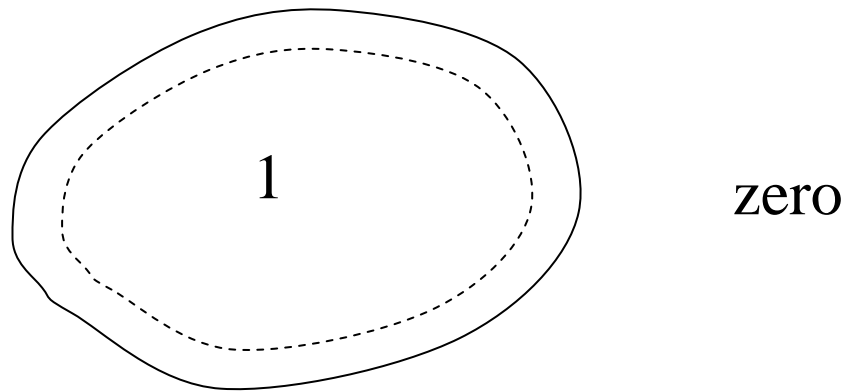
$$A \otimes B = \overline{\overline{A} \oplus \hat{B}}$$

- Frequently, B is symmetric and then reflection can be ignored



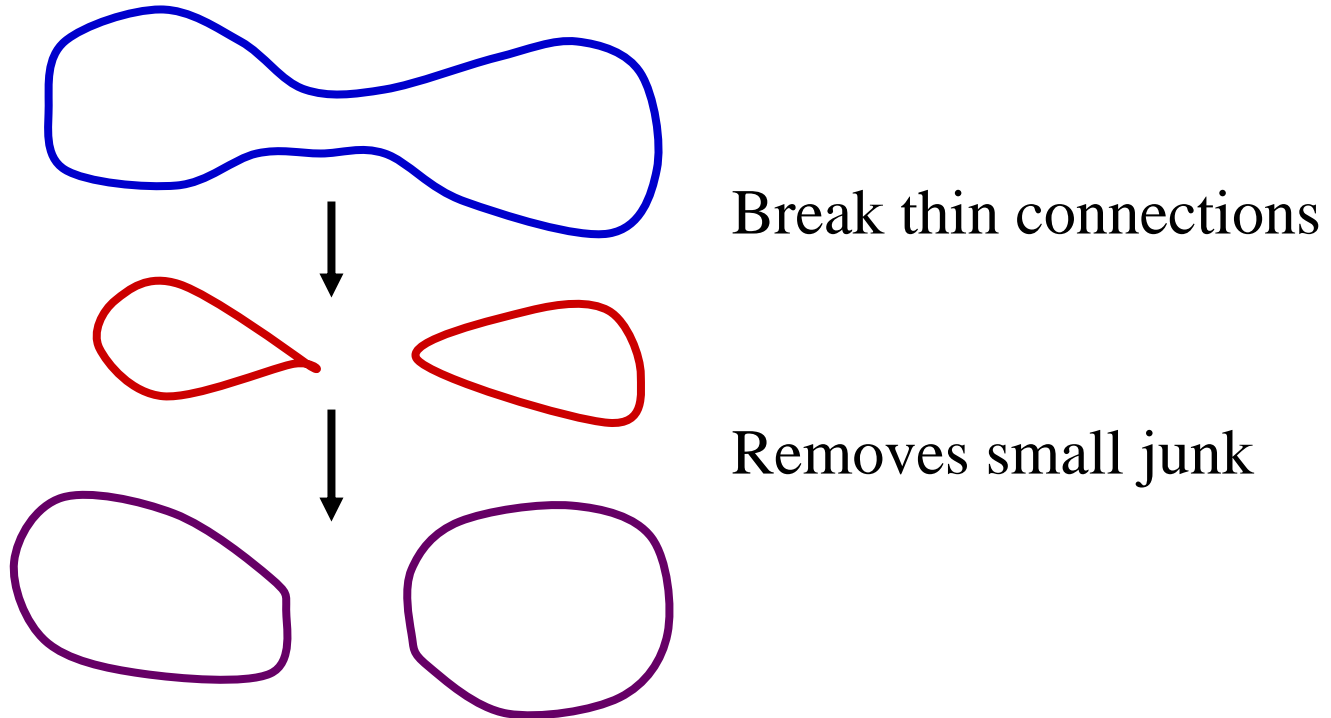
# Erosion

- Erosion by simple S.E.'s makes structures thinner
- Analog analogy:



# Opening

- Opening = Erode then Dilate



# Closing

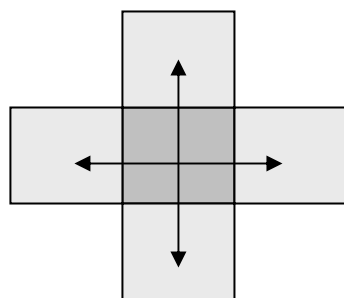
- Closing = Dilate then Erode
- Can attach objects that have become fragmented

# Erosion and Dilation

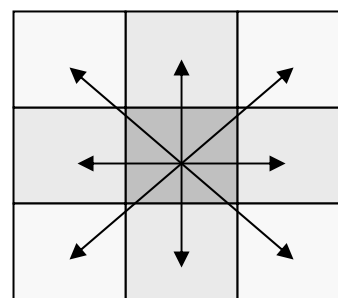
- Common trick in brain isolation “de-scalping”
  - Erode “it”
    - to disconnect brain from head
  - Dilate “it”
    - But *only* mark pixels that were originally “brain”

# Connectivity

- Define neighbor relation



4-neighbor



8-neighbor

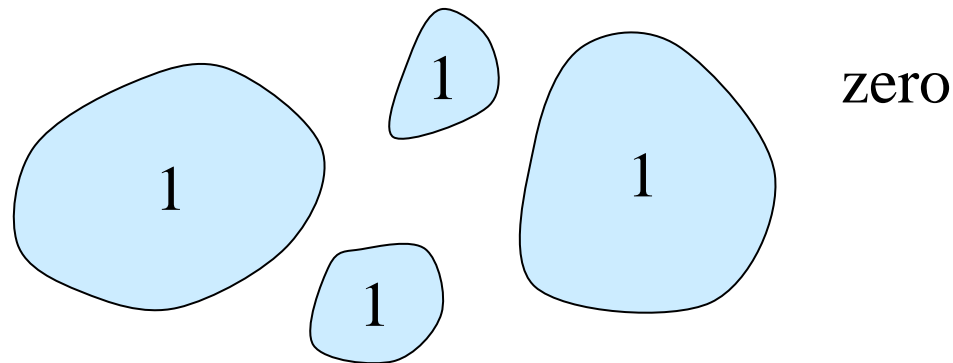
- There are some inconsistencies that a 6-neighbor relation can fix

# Finding Connected Components

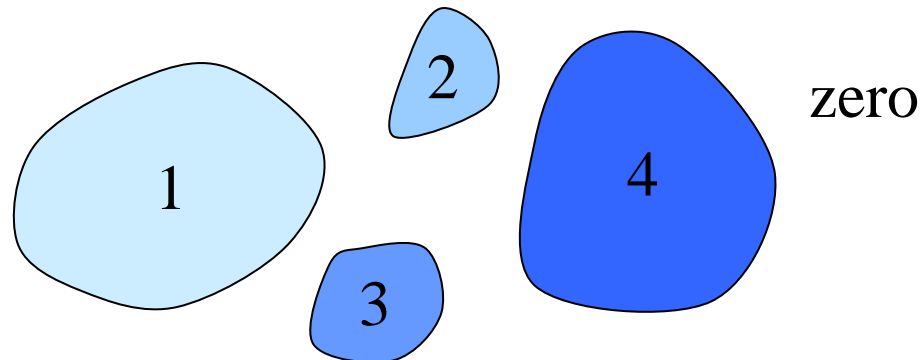
- $N = 1$
- Repeat until all pixels are labeled
  - Pick an unmarked  $I$  pixel
  - Label it, and all of its  $I$  neighbors,  $N$
  - $N \leftarrow N + 1$

# Connected Components: Example

- Boolean image



- Each separate object get a unique label



# Selected References

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